# 電機資訊學院 F BRAIN PLUS HAND 2024 冒實作專題競賽

## Hyper-beam Coherent Plane Wave Compounding for Improving Localization Accuracy of Ultrasound Localization Microscopy

Team : EECS004 Team member : Yen-Chen Wang

#### - I. INTRODUCTION

Diseases such as cardiovascular diseases, cancer, strokes and diabetes will make changes to capillaries in the early stages of the disease development. Thus, a way to image capillaries in vivo can speed up our research and prevention on these diseases.



Diameters of capillaries can be down to tens of micrometers, but ultrasound can only reach resolution up to hundreds of micrometers due to physical diffraction limitation.

To overcome limits, scientists developed an ultrasound imaging technique named Ultrasound Localization Microscopy (ULM) inspired by Photo-activated localization microscopy (PLAM).

We typically use low bubble density to avoid overlapping of PSFs, but it also causes longer data acquisition time.

In this research, we try solving this problem by introducing a new beamforming method hyperbeam coherent planewave compounding (HB-CPWC) with narrower PSF but similar computational time with coherent planewave compounding (CPWC).

#### ..... $\Box$ ..... plot the localized Final image with PLAM by Ground truth localize the original Imaging with few position in each frame summing all localized position in position of proteins protein location of each proteins excited by all frames PSF laser Steps of PLAM ⇒ Final image with ULM by plot the localized capillaries with micro-Imaging with localize the original summing all localized position ultrasound micro-bubble location of bubbles flowing in position in each in all frames each PSF frame them Steps of ULM

### - II. MATERIALS AND METHODS -

#### Hyper-beam Coherent Plane Wave Compounding (HB-CPWC)

- 1. In HB-CPWC, we divide the ultrasound transducer array into left and right subarrays.
- 2. By performing delay and sum on each subarray, we can obtain two beamsums  $S_L$  and  $S_R$
- 3. Calculate the sum of the two beamsums as  $S_S = |S_L| + |S_R|$ , as shown in Fig 1
- 4. Calculate the difference between the two beamsums as  $S_D = |S_L S_R|$ , as shown in Fig 2
- By subtracting S<sup>n</sup><sub>D</sub> from S<sup>n</sup><sub>S</sub> and taking the nth root, we achieve a much narrower PSF as shown in Fig 4 while comparing the PSF of CPWC showned in Fig 3





▲ Fig. 5 Root mean square error of HB-CPWC and CPWC under various SNR conditions. The RMSE values obtained with HB-CPWC were consistently lower than those obtained with CPWC across all tested signal-to-noise ratio (SNR) conditions

#### In Silico Flow Simulation : Testing Microvessel Resolvability



Fig. 6 Simulation results of V-shaped blood vessel with HB-CPWC and CPWC respectively under different bubble concentrations

0.26

Generate	Simulate RF data	Beamform the	localize the PSF in	Find minimal
scatterer	with Field II in	ultrasound images	each frame and	distance betweer
positions in each	each frame	with HB-CPWC and	track bubble	canals for us to
frame		CPWC respectively	trajectory between	determine a gap
			frames	

#### -IV. CONCLUSIONS

- 1. Here we propose a novel hyper-beam coherent plane wave compounding technique (HB-CPWC) which can produce narrower PSF while maintaining a computational complexity similar to that of the traditional coherent planewave compounding (CPWC) beamforming algorithm.
- 2. The results obtained from In Silico PSF simulations indicate that HB-CPWC can enhance microvessel localization accuracy and improve resolution compared to CPWC.
- 3. The improved microvessel distinguishability obtained from In Silico Flow simulations suggests that HB-CPWC can better differentiate closely positioned microvessels.



Bubble injection concentration (average bubbles/Sec)

▲ Fig. 7 Minimum separation distance with HB-CPWC and CPWC respectively under different bubble concentrations. The minimum distances achieved for identifying the two vessels with HB-CPWC consistently outperformed those achieved with CPWC across moderate bubble concentrations.